

Resting breathing contribution to the BOLD- and ADC-fMRI signals

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BACKGROUND

- **BOLD-fMRI** is an **indirect measure of neuronal activity** (neurovascular coupling), but can also be influenced by other components such as **respiration**, as shown in breath-hold tasks¹⁻³.
- Spontaneous changes in depth and/or rate of breathing happening during resting breathing can also cause significant changes in the BOLD signal^{1,2}.
- This can be related to **variations in arterial CO₂** (vasodilator)^{1,2} (as well as voluntary changes in breathing or chest motion induced B₀ inhomogeneities) and obscure true neuronal signals⁴.
- **ADC-fMRI** is a **neuromorphological** contrast sensitive to transient alteration of the apparent diffusion coefficient (ADC) resulting from **changes in tissue microstructure induced by brain activity**.
- We showed that the **ADC-fMRI is less sensitive to respiratory fluctuations**, and therefore **more specific to neuronal activity**.

METHODS

Acquisition:

- 2 sequences:
 - Isotropic ADC-fMRI (n=8), alternating b=200 (dfMRI-200) & b=1000 s mm⁻² (dfMRI-1000)
 - Multi-echo GE BOLD-fMRI (n=10)
- Parameters: TE=[12.6, 33.22, 53.84, 74.46] ms (BOLD)/105 ms (ADC), TR=1.1s, Matrix 82x82, 21 slices, resolution 2.8 mm isotropic, 40% slice gap, 192 s scan time
- Respiration (CO₂) recordings. End-tidal CO₂ (P_{ET}CO₂): interpolated signal from peaks detected at the end of exhaled breaths.

Processing :

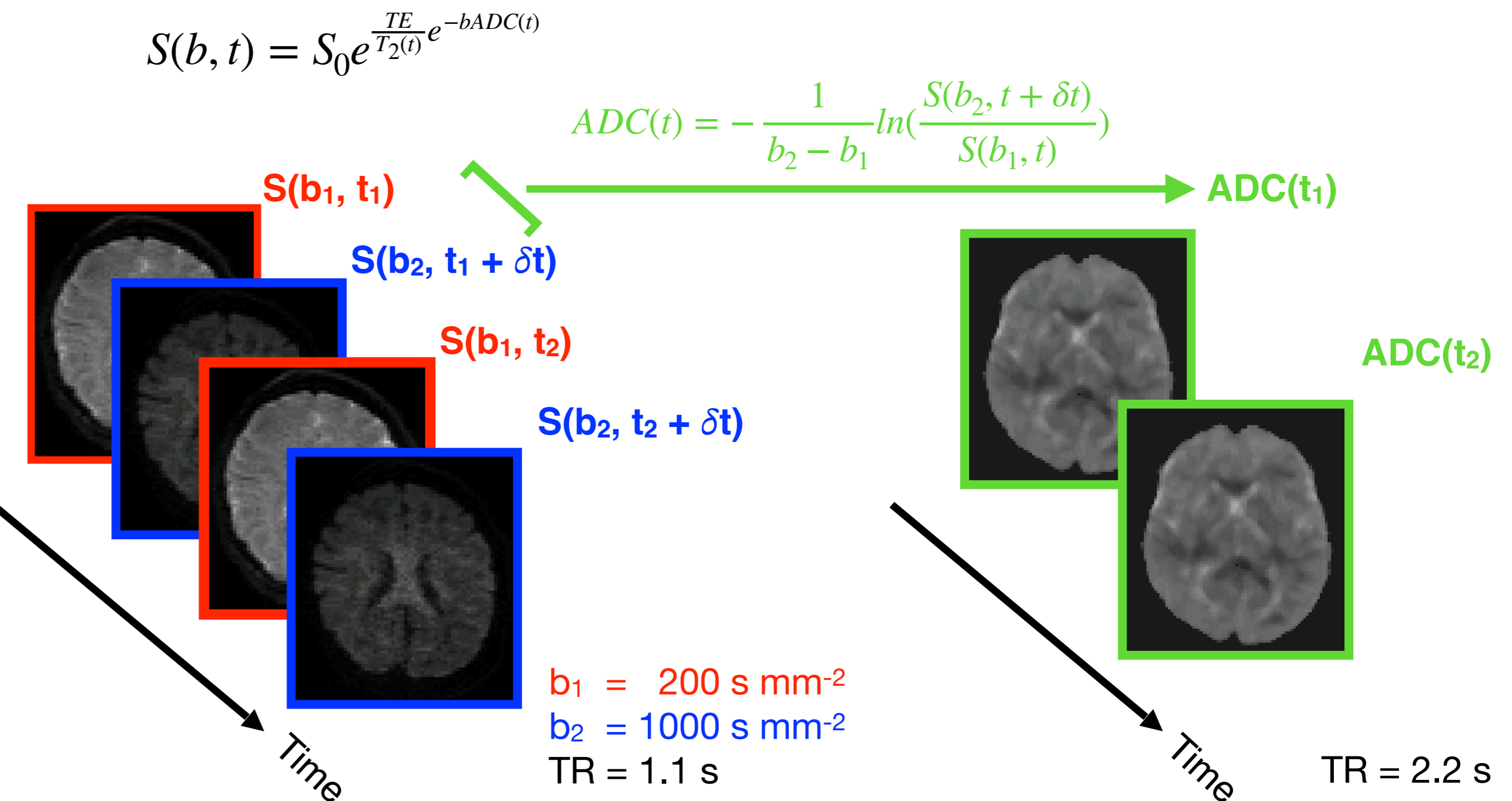
- Pre-processing as described in ref. 5
- MRI images: spatial filtering with Gaussian kernel (4 mm), high-pass temporal filter (4th order Butterworth, cut-off=0.01Hz)
- Physio time series: polynomial detrending (up to & including 3rd order polynomials), convolving with HRF³

Analysis:

- Cross-correlation (Pearson) P_{ET}CO₂ vs fMRI, lags= -24 to 0 s (steps of 1s).
- Significance threshold determination: null distribution approximation using surrogate analysis. For all subjects, generate 5000 surrogate P_{ET}CO₂ traces by shuffling the phases of the Fourier transformed P_{ET}CO₂, and run cross-correlation analysis with 5000 randomly selected voxels from the other subjects. The final null distribution pools all the subjects together.

DW-TRSE-EPI

$$S(b, t) = S_0 e^{-\frac{TE}{T_2^*(t)}} e^{-bADC(t)}$$



RESULTS

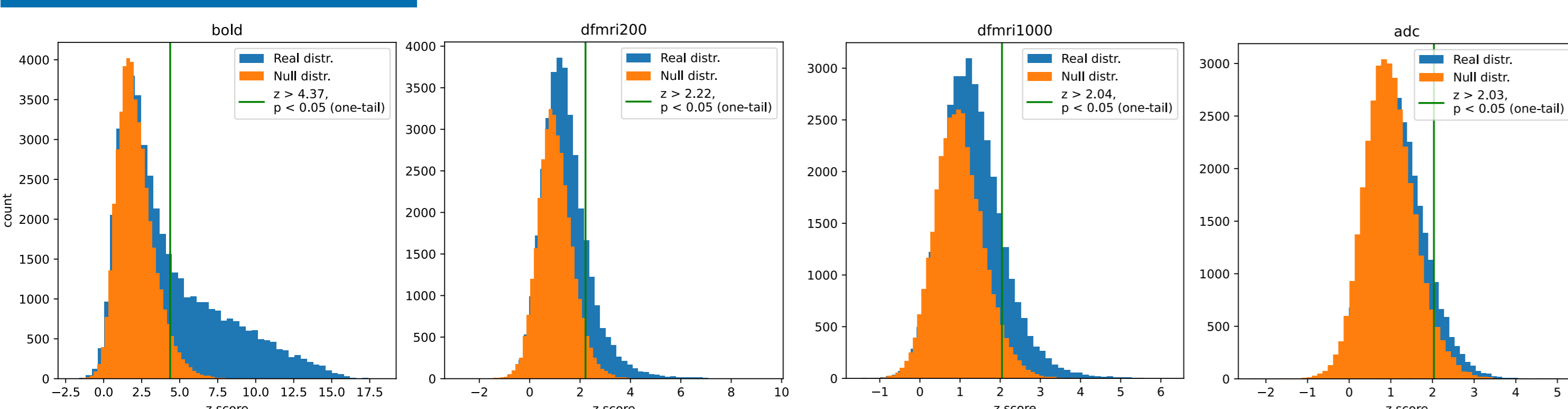


Fig. 1. Null distribution generated from surrogate signals, for BOLD, dfMRI-200, dfMRI-1000 and ADC signals.

- There is an increasing association between fMRI and P_{ET}CO₂ (Fig. 1-2): ADC < dfMRI-1000 < dfMRI-200 < BOLD
 - BOLD is heavily T₂*-weighted
 - dfMRI-200 suppresses blood water (small diffusion weighting) but is T₂-weighted
 - dfMRI-1000 similar to dfMRI-200 but more heavily diffusion-weighted
 - ADC suppresses both blood contribution and attenuates T₂-weighting
- GM vs WM (Fig. 2): despite reduced vasculature (↘ blood flow & volume) in WM^{6,7}, P_{ET}CO₂ is still strongly associated with BOLD-fMRI.
- Time lag maps (Fig. 3):
 - BOLD: delayed response in the WM, as already shown in ref. 8 with breath-hold. This is consistent with the heterogeneity of BOLD response as derived in ref. 9, which prevents the simultaneous mapping of GM & WM activity.
 - Diffusion-weighted: lags are mostly non-significant (no P_{ET}CO₂ vs fMRI association) & no pattern is visible.

CONCLUSION

- A clear association is found between resting breathing & BOLD
- Using diffusion-weighted signal decreases drastically this association → neuromorphological contrast is closer to neuronal activity than neurovascular contrast
- ADC-fMRI is robust to respiration-induced vascular changes and is therefore a promising tool to investigate neuronal activity in task^{-5,10} or rs-fMRI¹¹

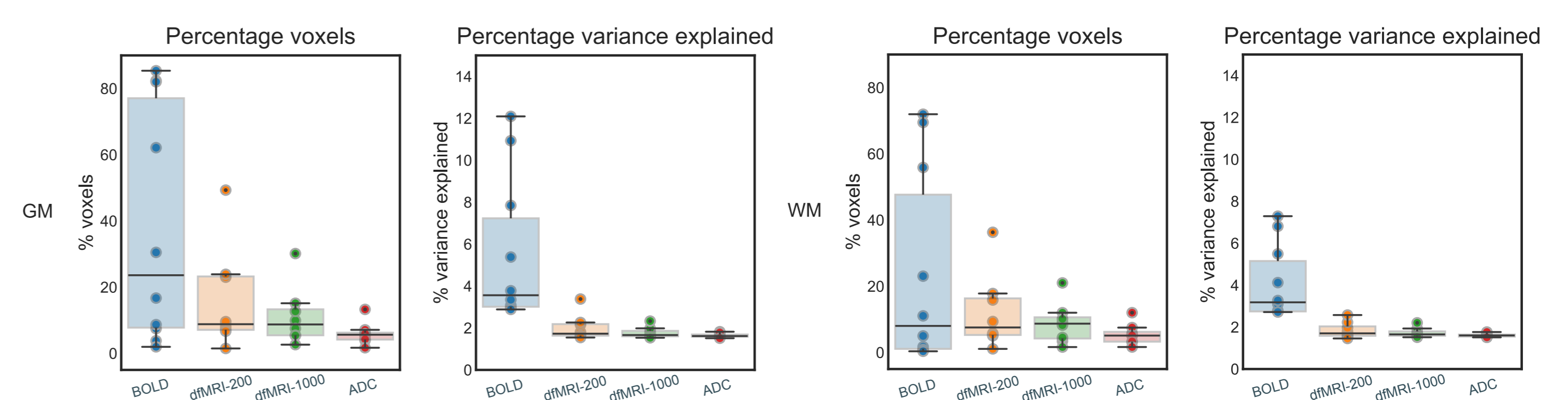


Fig. 2. Summary statistics of significant association between P_{ET}CO₂ and MRI signals, for BOLD, dfMRI-200, dfMRI-1000 and ADC signals. The statistics are shown in gray matter (GM) or white matter (WM) voxels which are above the significance thresholds derived in Figure 1.

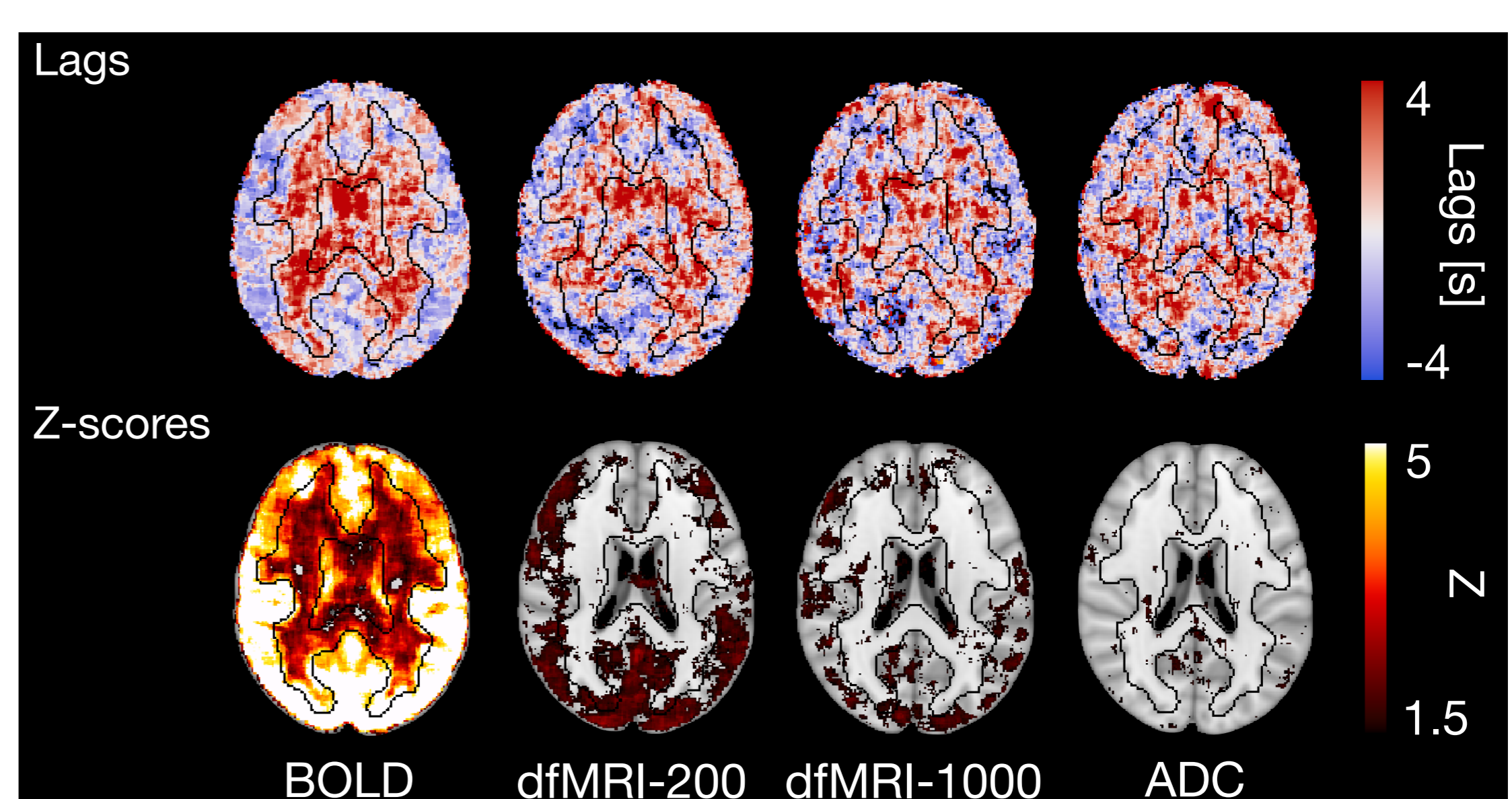


Fig. 3. Group-averaged time lag & z-score maps, for BOLD, dfMRI-200, dfMRI-1000 and ADC signals.

References:

- ¹Birn et al., NeuroImage, 2008, ²Chang and Glover, NeuroImage, 2009, ³Murphy et al., NeuroImage, 2011, ⁴Birn et al., NeuroImage, 2006, ⁵Spencer et al., bioRxiv, 2024, ⁶Biswal et al., Magn Reson Med, 1995, ⁷Gore et al., Magn Reson Imaging, 2019, ⁸Zvolanek et al., NeuroImage, 2023, ⁹Li et al., Nat Commun, 2019, ¹⁰Nguyen-Duc et al, bioRxiv, 2024, ¹¹de Riedmatten et al., bioRxiv, 2024